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11. Data were obtained from catalogs prepared separately for southern and eastern California (12), northern California before 1971 (13), and northern California after 1971 (14). A variety of magnitude scales have been used in California. For mainshocks ($M \geq 5.0$), M_W (moment magnitude) was used when available; otherwise M_L (local magnitude) was used. For southern and eastern California aftershocks, we used M_L for ($M \geq 3.0$), and M_{CA} (coda amplitude magnitude) for ($M < 3.0$). For northern California aftershocks, we used M_L before 1970 and M_D (coda duration amplitude) after 1970.
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15. This algorithm identifies clusters of earthquakes in time and space. By defining the identified clusters as the set of aftershocks, we effectively eliminate the spatial part of the problem. Thus, from this point on, the analysis considers aftershocks as two-dimensional (time-magnitude) vectors.
16. We used $c = 0.05$ days, the value that minimizes χ^2 for the post-1970 data.
17. Errors are ± 1 standard deviation of the mean.
18. Subsets of sequences occurring in each tectonic regime in California were compared with the two-sample t test for difference in the mean of each parameter; $\bar{a}_{\text{east}} > \bar{a}_{\text{north}}$, $p < 0.02$ and $\bar{a}_{\text{east}} > \bar{a}_{\text{south}}$, $p < 0.005$.
19. Sensitivity of the calculated probabilities to variations in the model parameters was investigated. A 10% increase in a , b , c , or p , relative to the generic value, leads to probabilities for strong aftershocks at $S = 1$, $(T - S) = 365$ of 0.44, 0.35, 0.32, and 0.25, respectively, compared to the generic probability of 0.32 in Table 1. Corresponding probabilities for larger mainshocks are 0.068, 0.042, 0.046 and 0.035, compared to the generic probability 0.046 in Table 1.
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30. The empirical (isotropic) spatial distribution of strong aftershocks in California was determined from the California data. The median distance between $M \geq 5.0$ aftershocks and their mainshock epicenter is 5 km. The 80 percentile distance is 9 km.
31. We thank M. V. Matthews for providing technical assistance throughout the study, B. Ellsworth and Y. Ogata for helpful discussions and suggestions, and R. D. Brown, for initially stimulating our interest in this problem.

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Time and Spatial Dependence of the Concentration of Less Than 10^5 Microelectrode-Generated Molecules

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The time and spatial dependence of the concentration of as few as 40,000 electrogenerated, redox-active molecules has been determined. The distance between generator and detector microelectrodes in an array used in the study could be varied from 0.8 to 28 micrometers. Measurements of a sufficiently small ensemble of molecules allowed the experimental results to be compared with a quantitative simulation of the random movement of each member of the ensemble. The transit time of an electrogenerated species from the generator to a collector microelectrode was measured as a function of viscosity, diffusivity, and distance.

MICROELECTROCHEMICAL DEVICES can be used in the study of catalysis, energy conversion, sensors, displays, and molecule-based electronics (1-4). In 1984 Kittlesen and Wrighton introduced the microfabrication of arrays of closely spaced, individually addressable micrometer-dimensioned electrodes (5) and their subsequent modification to fabricate molecule-based transistors, diodes, and sensors (6). In biological systems in which electrochemical stimulation or monitoring is useful, such as in the release of drugs and neurotransmitters (7), the use of microelectrodes may prove useful for creating and monitoring chemical signals. Another goal of such research is to reduce the size of the ensemble of electrogenerated species so that discrete electrochemical events can be measured.

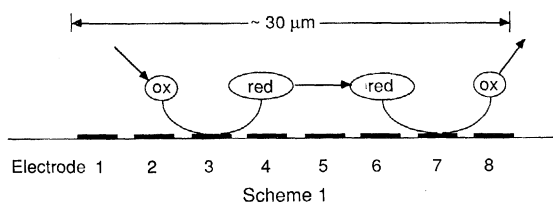
We have used an array of closely spaced ($\sim 1 \mu\text{m}$), individually addressable micro-

electrodes ($<10^{-7} \text{ cm}^2$ in area) to monitor the time and spatial dependence of $<10^5$ electrogenerated species. We have directly measured the dynamics associated with diffusing species on a sufficiently small scale ($<30 \mu\text{m}$) and of sufficiently few species ($<10^5$) that the measurements can be compared with a quantitative simulation of the random movement of each species. Studies of the dynamics of electrogenerated species in the solid state and other media not accessible by traditional electrochemical methods, such as rotating ring-disk electrodes, should now be possible (8).

Electrochemical methods have been used to monitor the diffusion of electrogenerated species. The concentration profile within the diffusion layer near a macroelectrode can be mapped to within $\sim 5 \mu\text{m}$ with a movable light source (9) or a movable microelectrode (10). Microelectrodes have been used to monitor the time of flight of a pulse of 10^{-6} C through a variety of thin films overcoating the microelectrodes (11). Our smaller microelectrodes allow these diffusion studies to be extended to a qualitatively smaller amount of electrogenerated material.

Recently, Bard *et al.* demonstrated that in steady-state experiments a large fraction of redox-active material generated at one microelectrode can be detected or "collected" at nearby microelectrodes (12). We show here that the transit time for movement of the electrogenerated species from generator to collector is a measure of the diffusion characteristics of the electrogenerated solution species. A redox-active species is generated at one electrode, diffuses, and is collected at a second electrode (Scheme 1). Procedures used in the microfabrication and pretreatment of the gold microelectrode arrays are similar to those described in (13, 14).

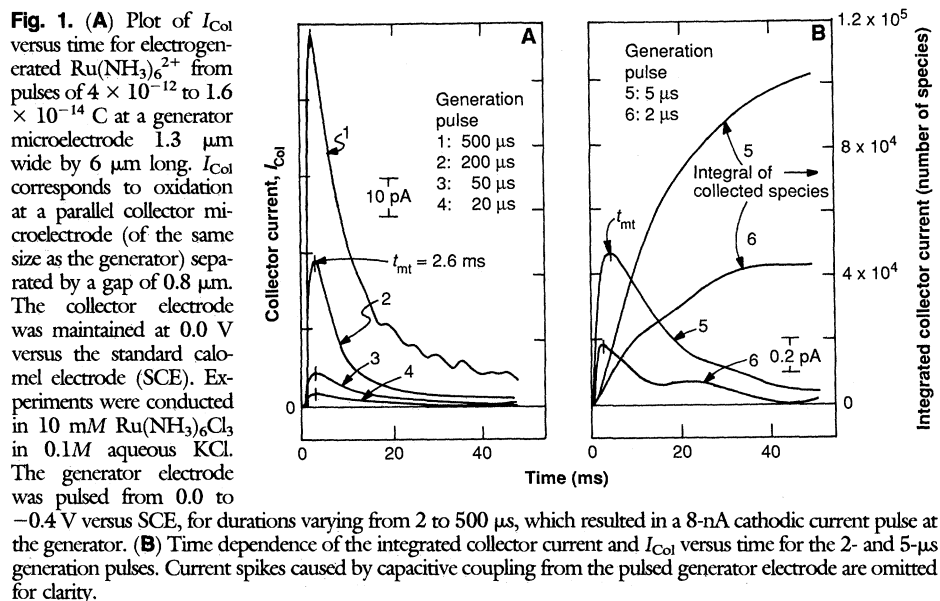
The experimental in situ spatial and tem-



Scheme 1. Representation of generation-collection experiments at a microelectrode array where "generation" can be effected at any one of the microelectrodes and "collection" can be done at any other microelectrode. The potential at electrode 3 is pulsed to "generate" an ensemble of reduced species. The potential at electrode 7 is fixed to "collect" a fraction of the reduced species by oxidation.

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poral distribution of electrogenerated redox-active species is illustrated with measurements of the generation (Eq. 1) and collection (Eq. 2) of $Ru(NH_3)_6^{2+}$:



The microelectrode array is immersed in an electrolyte solution containing $Ru(NH_3)_6^{3+}$ as the only active species. Initially, microelectrodes termed "generator" and "collector" are maintained at E_{ox} , a potential positive of E' [$Ru(NH_3)_6^{3+/2+}$]. The generator is then pulsed to a reducing potential, E_{red} , which creates $Ru(NH_3)_6^{2+}$ in a process that is monitored by a cathodic current I_{Gen} . Of the generated $Ru(NH_3)_6^{2+}$, 71% escapes from the generator in a pulse from E_{ox} to E_{red} and back to E_{ox} (8). As the $Ru(NH_3)_6^{2+}$ diffuses away from the generator, the time variation of the current at the collector, I_{Col} , signals the arrival, collection, and regeneration of $Ru(NH_3)_6^{3+}$. Alternatively, movement of $Ru(NH_3)_6^{3+}$ may be studied through the application of an oxidizing potential in an electrolyte that initially contains only $Ru(NH_3)_6^{2+}$. Our results demonstrate that I_{Col} is proportional to the concentration of the relevant redox species, so that the time dependence of I_{Col} at a given collector yields time-dependent concentration data for the electrogenerated species. Independent measures of I_{Col} versus time at different collectors allow mapping of the spatial dependence of the concentration at a given time.

Typical measurements of I_{Col} versus time are presented in Fig. 1 for $Ru(NH_3)_6^{2+}$ generated with square-wave pulses and collected at two microelectrodes separated by $0.8 \mu m$. The collection efficiency Φ_{ss} , which

is the ratio of collected species to generated species (12), is ~ 0.40 (independent of generation pulse time) from the integrated I_{Col} . The time dependence of the collection of as little as 7×10^{-20} mol, or $40,000$ $Ru(NH_3)_6^{2+}$ ions, is shown. The relevant dynamic parameter is the transit time, t_{mt} , which is taken to be the time at which one observes the maximum value of I_{Col} . We can routinely measure I_{Col} as low as 10^{-13} A to a time resolution of 1 ms, which gives an integrated resolution of 10^{-16} C (10^{-21} mol, or less than 1000 ions). By taking $t = 0$ to be the midpoint of the generation pulse, we find that t_{mt} is 2.6 ± 0.3 ms (range from sets of 10 independent trials) for the 0.8 - μm gap between generator and collector electrodes and is independent of the generator pulse time. We used typical generator pulse times that were less than one-third of the expected value of t_{mt} to reduce complications from "feedback" (12).

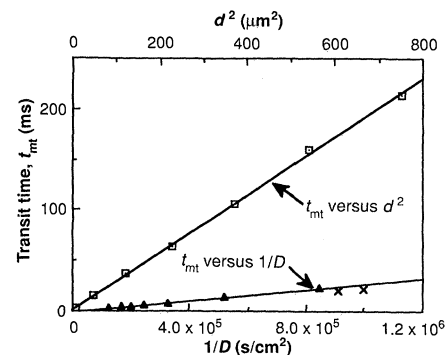
Data in Fig. 1 illustrate the concept of pulsed generation-collection experiments, but complications in relating t_{mt} to the diffusivity occur in that the width of the generator microelectrode ($1.3 \mu m$) is greater than the gap ($0.8 \mu m$) separating it from the collector. We related t_{mt} to diffusivity by measuring t_{mt} for transit across an array of seven collector microelectrodes (Fig. 2). Each one of the eight microelectrodes is $2.7 \mu m$ wide, and they are separated from each other by $1.4 \mu m$. We adjusted the distance d , the separation from the center of the generator to the nearest edge of the activated collector, by collecting at one of the seven collector electrodes. For the $Ru(NH_3)_6^{3+/2+}$ experiments, the plot of t_{mt} versus d^2 was essentially linear, as expected for diffusion. For a diffusional process, t_{mt} should be

proportional to $1/D$. By varying the sucrose content of the aqueous $Ru(NH_3)_6^{3+/2+}$ solution, we varied D in a systematic fashion (15). Results of measurements of t_{mt} for several sucrose solutions (Fig. 2) show that $t_{mt} \propto 1/D$. An absolute value of D for $Ru(NH_3)_6^{2+}$ in 0.1 M $NaClO_4$ was determined from limiting currents at a 25 - μm microdisk electrode. Thus the $Ru(NH_3)_6^{3+/2+}$ experiments are consistent with Eq. 3:

$$t_{mt} = 0.22 d^2/D \quad (3)$$

The constant of proportionality for an array of parallel "band" microelectrodes is 0.22 ± 0.02 . Thus, for this geometry, t_{mt} can be used with Eq. 3 to determine D . The concentration of the diffusing species need not be accurately known with this method.

Cytochrome c illustrates how our technique can be used to measure D . This molecule has been characterized by the spreading of the sedimentation boundary of an ultracentrifuged sample (16), cyclic voltammetry (17), and rotating disk voltammetry (18). Although the generally accepted value of D for cytochrome c is 1.1×10^{-6} cm^2/s , values from various modified electrode methods span the range from 1.8×10^{-7} to 11×10^{-7} cm^2/s (17–20). Our technique is a direct measurement and should be independent of the electrode material used. Our t_{mt} values for ferrocyanide yielded $D = 1.1 \times 10^{-6}$ cm^2/s , consistent with the accepted values obtained with rotating disk



voltammetry (18) and chronoabsorptometry (20) (Fig. 2). We also found $D = 1.0 \times 10^{-6} \text{ cm}^2/\text{s}$ for ferricytochrome c. Because the relative errors in our measurements are sufficiently small, we conclude that there is an experimentally significant difference for D between the reduced and the oxidized forms of cytochrome c.

We were interested in quantitatively simulating generation-collection experiments in order to better understand the concentration evolution with time. However, in the analysis of mass transport to and from small electrodes, discontinuities occur at the microelectrode edges where the diffusion-limited flux for a reversible system is infinite (21). Thus, we chose to describe the diffusion numerically with the simpler Einstein-Smoluchowski random walk rather than analytically with Fick's laws. A two-dimensional digital simulation (in the plane normal to the array) was used. Simulated concentration profiles of the generated species are shown in Fig. 3 for a generation-collection experiment similar to that summarized by data in Fig. 2. The simulation accurately describes the variation in Φ_{ss} values upon changes in (i) collector symmetry, (ii) collector width, (iii) distance

from the generator electrode, and (iv) diffusion coefficient. Subsequent to a generation pulse, the peak of I_{Col} (the maximum collection rate) occurs at a time t_{mt} according to Eq. 4 for band microelectrodes:

$$t_{\text{mt}} (\text{simulation}) = (0.20)d^2/D \quad (4)$$

The simulation size, 10^4 random particles, closely approximates the actual number of species generated in our experiments. The simulation accurately predicts our experimental determination of the D and d dependence of t_{mt} (Eq. 3) (14).

Our studies demonstrate an experimental and theoretical methodology suitable for investigating the diffusion of redox-active molecules in solution. If the interelectrode separation is reduced to $<0.1 \mu\text{m}$ by shadow deposition techniques (22), the values of t_{mt} should decrease by a factor of ~ 100 , whereas the peak value of I_{Col} should increase by the same factor for a given number of generated species. In principle, our measurements of $\sim 40,000$ species (Fig. 1B) could be extended to as few as several hundred. Smaller interelectrode spacings would also allow more convenient measure of D for situations where D is small, as in solid-state electrolytes (23). Because D and solu-

tion viscosity are related according to Eq. 5 (24), measurements of t_{mt} allow determination of viscosity, η ,

$$D = z_i e_0 / 6 \pi k T r \eta \quad (5)$$

where z_i is the charge on the ion, e_0 is the fundamental unit of charge, k is Boltzmann's constant, T is temperature, and r is the Stokes radius of the ion. Such arrays may be useful in probing local versus global viscosity (25). For polymers, solid electrolytes, and gels, our techniques should provide useful information on the diffusivity and local environments of redox-active materials for which hydrodynamic techniques (8) may not be suitable.

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